Gender-variability of minimum foot clearance during walking in adults and elderly

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Versão Definitiva

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Abstract

Falls are a public health problem faced by many countries representing a heavy burden for societies, particularly for those in which the population is aging. In fact, a high risk of falls is associated with older age groups. The increased frequency of falls in the elderly is responsible for many deaths and unintentional accidents impacting negatively their quality of life. It has been suggested that women are at a higher risk of falling than men, although little is known whether the factors that affect the risk of falls vary between men and women. The minimum foot clearance and its variability is an important parameter of gait which can be related to the mechanism of falls.

The present study aims to investigate older adults’ gender-related differences in minimum foot clearance, particularly its variability/complexity during walking. This study included 43 physically active subjects, of whom 23 were women and 20 were men. Participants walked on a treadmill for 14 minutes at a preferred walking speed. Minimum foot clearance data were obtained through a 3D motion capture system using 8 infrared cameras at a sampling frequency of 100 Hz. Sixteen retroreflective markers of 10 mm were placed on the anatomical landmarks of the right and left sides according to the recommendations of the Plug-in-Gait Lower Body model. Three additionally half markers of 10 mm were placed into each shoe for proper determination of minimum foot clearance, during gait.

The results showed that women had a lower mean in the minimum foot clearance (11.63 mm) compared to men (14.84 mm). Regarding the complexity of the minimum foot clearance, no gender differences were found. In conclusion, although men and women had similar complexity of minimum foot clearance, the women exhibited a minimum foot clearance mean lower than men, which may increase their risk of falling.

Keywords

Minimum foot clearance, Complexity, Gait, Older adults, Falls
Resumo

As quedas são um problema de saúde pública enfrentado por muitos países representando um fardo pesado para as sociedades, particularmente para aquelas em que a população está a envelhecer. De fato, altos riscos de queda estão associados a grupos etários mais velhos. O aumento da frequência de quedas nos idosos é responsável por muitas mortes e acidentes não intencionais com impacto negativo na sua qualidade de vida. Tem sido sugerido que as mulheres correm maior risco de cair do que os homens, embora pouco se saiba se os fatores que afetam o risco de quedas variam entre homens e mulheres. A distância vertical mínima do pé bem como a sua variabilidade é um parâmetro importante na marcha que se relaciona com o mecanismo de queda.

O presente trabalho teve como objetivo investigar diferenças de género em adultos e idosos na distância vertical mínima do pé, particularmente a sua variabilidade/complexidade durante o caminhar. Fizeram parte deste estudo 43 sujeitos fisicamente ativos, dos quais 23 eram mulheres e 20 homens. Os participantes caminharam numa passadeira rolante durante 14 minutos, à sua velocidade natural de caminhar. Os dados da distância vertical mínima do pé foram obtidos através de um sistema de captura de movimento 3D usando 8 câmaras de infravermelho com uma frequência de amostragem de 100 Hz. Dezasseis marcas retrorrefletoras de 10 mm foram colocadas nos pontos anatômicos do lado direito e esquerdo do participante de acordo com as recomendações do modelo Plug-In-Gait Lower Body. Três marcadores adicionais de 10 mm foram colocados em cada sapato para a determinação adequada da distância vertical mínima do pé, durante a marcha. Os resultados permitiram verificar que as mulheres possuem uma menor média na distância vertical mínima do pé (11.63 mm) em comparação com os homens (14.84 mm). Em relação à complexidade da distância vertical mínima não foram encontradas diferenças de género.

Em conclusão, embora homens e mulheres tenham uma complexidade da distância vertical mínima do pé semelhante, as mulheres apresentam uma menor média na distância vertical mínima do pé, o que pode aumentar o seu risco de queda.

Palavras-chave

Distância vertical mínima, Complexidade, Caminhar, Idosos, Quedas
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List of Abbreviations

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<th>Description</th>
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<tr>
<td>DFA</td>
<td>Detrended Fluctuation Analysis</td>
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<td>MFC</td>
<td>Minimum Foot Clearance</td>
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<td>PWS</td>
<td>Preferred Walking Speed</td>
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Chapter 1. Introduction

The world's population is aging and according to the United Nations, by 2050, the elderly population will increase to 2 billion people (World Health, 2008). Biological degeneration associated with aging has been linked to the risk of falls. The frequency of falls can increase threefold in older adults because of the loss of muscle mass and strength (Landi et al., 2012). Falls can cause moderate to severe injuries, compromise mobility, lead to loss of independence, hospitalizations and sometimes even death (Chiba, Ebihara, Tomita, Sasaki, & Butler, 2005; Prince, Corriiveau, Hébert, & Winter, 1997). Falls occur frequently in the older population during walking, with about 53% of falls in older adults occurring when stumbling due to involuntary contact of the foot with the ground or with an obstacle (Blake et al., 1988). Due to the serious consequences and the high health expenses associated with falls the recognition of potential fallers is essential (Stevens, Corso, Finkelstein, & Miller, 2006).

It has been suggested that women show higher risk of fall than men (Gale, Cooper, & Aihie Sayer, 2016; Grisso, Schwarz, Miles, & Holmes, 1996). Non-fatal falls related injuries are also more common among older women (Stevens & Sogolow, 2005). Ninety percent of hip fractures are caused by falls, making this type of injury an important predictor of falls (Ambrose, Paul, & Hausdorff, 2013), and women show a substantially greater number of hip fractures than men (Stevens & Sogolow, 2005). Gender differences can also be related with the activities performed, for instance older adults have significantly higher rates of falls when outdoors doing specific physical activities, while women (Duckham et al., 2013) are at increased risk of fall and get injured when performing indoor activities.

Minimum Foot Clearance (MFC) is thought to be a parameter related with the risk of tripping and falls (Begg, Best, Dell'Oro, & Taylor, 2007; Winter, 1992) that occurs when the horizontal velocity of the foot is close to its maximum (Winter, Patla, Frank, & Walt, 1990), which supposedly may enhance the risk of trip and fall (Khandoker, Lynch, Karmakar, Begg, & Palaniswami, 2010). MFC is defined as the minimum vertical distance between the anterior part of the foot/shoe and the ground during the mid-swing phase (Karmakar, Khandoker, Begg, & Palaniswami, 2013). Interestingly, sex-related differences were found during this phase of gait. For instance, older men showed increased rectus femoris muscle activation during the mid-swing phase, while women show greater gastrocnemius lateralis activation (Bailey et al., 2018). Lower knee joint flexion angle was reported in women when compared to men from the late stance to mid-swing before and after knee arthroplasty surgery (Wilson, Dunbar, & Hubley-Kozey, 2015). The duration of dorsiflexion during the initial swing also increased less abruptly with age for men than for women (Ko, Tolea, Hausdorff, & Ferrucci, 2011). Differences in hip and knee angles were also found between women and men (Boyer,
Beaupre, & Andriacchi, 2008; Hurd, Chmielewski, Axe, Davis, & Snyder-Mackler, 2004). All these gender-related differences suggest that MFC can be affected differently across sexes, which demands further clarification. Moreover, reduced MFC is believed to indicate an increased risk of tripping (Rosenblatt, Bauer, & Grabiner, 2017). Notably, after an intervention in stroke patients the increase in MFC was accompanied by a reduction in falls (Gervasoni et al., 2017).

Recently, it has been shown that MFC can either increase or decrease depending on the environmental constraints. A cognitive task during walking reduced MFC while visual restriction led to increased MFC (Killeen et al., 2017). It has been suggested that MFC, as a single time point measure within the gait cycle, may provide limited insights to risk of falls, for example, Byju, Nussbaum, and Madigan (2016) suggested that using more information from the toe’s trajectory can better predict the probability of tripping. The major limitation of the measures employed in these studies is that the relationship between consecutive steps is largely ignored, and the temporal structure of the time series is disregarded. However, healthy normal walking exhibits persistent long-range correlations where each step over a large time series is correlated with the previous and with next step (J. M. Hausdorff, Peng, Ladin, Wei, & Goldberger, 1995).

Human movement variability is thought to be an intrinsic and fundamental characteristic of human walking, denoting the variations in a movement pattern when the same task is repeated multiple times (Stergiou, Kent, & McGrath, 2016). It has been suggested that and optimal level of variability is associated with healthy states while too much or too little variability represents an unhealthy and less adaptable system (Stergiou, Harbourne, & Cavanaugh, 2006). Random (too much variability) and periodic (too little or no variability) systems are characterized by a loss of complexity, indicating that a system is either too unstable or rigid and, hence less adaptable (Stergiou et al., 2006). Healthy gait has shown to be complex (Hunt, McGrath, & Stergiou, 2014; Kaipust, McGrath, Mukherjee, & Stergiou, 2013), while the gait of older adults (Kaipust et al., 2013) and neurological patients (J. M. Hausdorff, 2009) showed a loss of complexity.

Mills, Barrett, and Morrison (2008), studied MFC variability during treadmill walking in young and elderly men and reported that the elderly shows greater MFC variability, even though the p-value was 0.049. Similarly, greater MFC variability was reported, but only for the right leg of older men when compared to young men (Sparrow, Begg, & Parker, 2008).

When MFC variability was investigated between young and elderly females, higher variability was also found for elderly (Begg et al., 2007). In addition to the small number of individuals (ranging from 10 to 16 per group) who participated in these studies, variability was assessed through linear measures of central tendency, which have been reported to show shortcomings (Buzzi, Stergiou, Kurz, Hageman, & Heidel, 2003). Particularly because, the dynamics that
underlie the control of locomotion are non-linear and complex (Harbourne & Stergiou, 2009; J. M. Hausdorff et al., 1995). However, linear statistics lack the ability to provide information about complexity and consequently valuable information can be lost.

In the non-linear context, a decrease in MFC complexity was also found in older adults with history of falls when compared to healthy elderly and young subjects (Karmakar et al., 2013). However, to the best of the authors’ knowledge, no studies have evaluated MFC variability regarding gender-related differences and its implications concerning the risk of falls.

Therefore, the present study aims to investigate older adults’ sex-related differences in minimum foot clearance. Based on previous findings, it was hypothesized that: 1) minimum foot clearance will be smaller in women and; 2) women will exhibit decreased complexity of minimum foot clearance compared to men.
Chapter 2. Methods

Participants
The demographics of 43 subjects (23 women, 20 men) who participated in the study are shown in Table 1, as well as, spatiotemporal gait variables. The body mass and height of each participant were measured by a conventional scale and stadiometer, respectively. The subjects were physically active and performed exercise sessions of 45 minutes at least 2 times per week. Each subject was controlled through questionnaire for the following conditions: history of falls during the last 12 months, stroke, recent surgery, myopathy, neuropathy, scoliosis, arterial disease, rheumatoid arthritis, diabetes, lower limb injury in the last 6 months, joint replacement, pulmonary and/or cardiac diseases, asthma, acute pain, foot deformities and locomotor disorders.

Written informed consent was obtained from all participants and the study was approved by the Ethics Committee of University of Beira Interior.

<table>
<thead>
<tr>
<th>Variables</th>
<th>Age (years)</th>
<th>Mass (kg)</th>
<th>Height (m)</th>
<th>Gait Velocity (km/h)</th>
<th>Cadence (steps/min)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Women (n = 23)</td>
<td>65.8 ± 4.6</td>
<td>66.0 ± 9.3</td>
<td>1.54 ± 0.04</td>
<td>3.7 ± 0.4</td>
<td>113.0 ± 9.3</td>
</tr>
<tr>
<td>Men (n = 20)</td>
<td>61.9 ± 5.3</td>
<td>77.1 ± 9.0</td>
<td>1.69 ± 0.07</td>
<td>3.8 ± 0.5</td>
<td>105.5 ± 10.2</td>
</tr>
<tr>
<td>Total (n = 43)</td>
<td>64.0 ± 5.4</td>
<td>71.2 ± 10.6</td>
<td>1.60 ± 0.10</td>
<td>3.8 ± 0.1</td>
<td>109.5 ± 1.6</td>
</tr>
</tbody>
</table>

Experimental Procedures
The procedures took place into two stages, in the first the Preferred Walking Speed (PWS) was estimated in the treadmill (h/p/cosmos Mercury 4.0, Munich, Germany) and in the second stage the subjects went to the lab, after a week of PWS assessment, for MFC measurements. After a familiarization period (i.e. 10-min) in the treadmill the PWS was estimated as follows:
1) From 1.5 km/h the initial speed was increased in intervals of 0.1 km/h at every six strides until the participant informed that the speed was uncomfortable, the value immediately prior to this speed was considered the maximum speed;
2) The reverse procedure was then performed by reducing the speed in steps of 0.1 km/h until the participant reported that the speed was very low, the value immediately prior to this speed was considered the minimum speed (Karmakar et al., 2013).

The subjects were not aware of the treadmill speeds being applied. This procedure was performed 6 times, and the mean of the 6 maximum and 6 minimum speeds was considered the PWS. In the second stage and after a familiarization period (i.e. 3-min) participants
walked for 14 minutes, at the PWS previously estimated, to ensure the minimum number of recommended walking cycles (i.e. 600) in time series analysis (Damouras, Chang, Sejdic, & Chau, 2010).

The MFC data were obtained through the 3D motion analysis system using 8 infrared cameras Mx T20-S (Vicon Motus, Oxford, UK) at a sampling frequency of 100 Hz. Sixteen retroreflective marks of 10 mm were placed on the anatomical landmarks of the right and left sides according to the recommendations of the Plug-in-Gait Lower Body model (Vicon Motus, Oxford, UK). Three additionally half markers of 10 mm were placed into each shoe (Figure 1) for proper determination of MFC. Equal shoes of different sizes were purchased for the study, to ensure accurate determination of the MFC and that the tests were not affected by the type of shoe used (Annette M. Davis, Brook Galna, Anna T. Murphy, Cylie M. Williams, & Terry P. Haines, 2016). The markers were glued on the front rubber of the footwear and aligned with the first, third and fifth metatarsal (i.e. M1, M3, and M5), as shown in Figure 1.

![Figure 1 - Position of the three retroreflective markers used to determine MFC. The markers were aligned with the metatarsals 1, 3 and 5 (i.e. M1, M3 and M5).](image)

Before assess walking data, a static trial was collected, in which it was ensured that the entire sole of the shoe was in contact with the ground. Based on the static trial the vertical distance of each marker (i.e. M1, M3 and M5) to the ground was then measured with the software Nexus 2.6 (Vicon Motus, Oxford, UK) for each subject. This vertical distance was then subtracted from the MFC height calculated from the dynamic trials, as shown in Figure 2, to obtain the correct MFC distance (i.e. the vertical distance between the sole of the shoe and the ground). The MFC was determined from unfiltered data for each of the three markers placed on the shoe (i.e. M1, M3 and M5) and the marker that showed the smallest MFC value was used in subsequent analysis (Khandoker et al., 2010).
Statistical procedures

Scaling properties are important to determine the complexity of a time-series, which can be accessed through Detrended Fluctuation Analysis (DFA). In this context the MATLAB software (MATLAB R 2018a, MathWorks, Inc., Natick, MA, United States) was used to perform DFA and estimate the self-similarity scaling parameter \( \alpha \). Several stages are used to determine the scaling exponent \( \alpha \).

Briefly, DFA is used to identify fractal-like (i.e. self-similar), processes by integrating data over time where each time series integrated will be self-similar if the fluctuations at different time windows \( [F(n)] \) scale as a power-law with window size \( n \). A linear relationship on a double-log graph will denote self-similarity with \( F(n) = n^\alpha \), while the slope of the gradient, relating the log \( F(n) \) to the log \( n \), will determine the scaling parameter \( \alpha \) (Jeffrey M. Hausdorff, 2007). If a value of MFC during a stride does not correlate with previous values we are in the presence of white noise, and the fractal index would be \( \approx 0.5 \). An \( \alpha \approx 1.5 \) (i.e. brown noise) indicates deterministic structure within the MFC correlations, while \( \alpha \approx 1.0 \) (i.e. 1/f noise) shows stochastic properties within the MFC time series which have a fractal self-similar structure. The size of the windows used was 16 to \( N/9 \), while the \( N \) considered was 800 to comply with the minimum number of recommended walking cycles (i.e. 600) (Damouras et al., 2010).

After determining the scaling exponent \( \alpha \) using DFA, statistical analysis of two dependent variables (MFC mean and MFC \( \alpha \)) was performed employing the independent-samples t-test to evaluate if there were differences between men and women. Engagement scores for each level of gender were normally distributed, as assessed by Shapiro-Wilk's test (\( p > 0.05 \)), and there was homogeneity of variances, as assessed by Levene's test for equality of variances (\( p = 0.138 \)). A \( p < 0.05 \) was considered statistically significant and the data were analyzed using SPSS (IBM SPSS Statistics 25.0, Chicago, IL, USA).
Chapter 3. Results

The following dependent variables (MFC mean and MFC $\alpha$) were compared between men and women, through independent-samples t-test. As summarised in Table 2 women showed significant smaller MFC mean (11.63 mm) than men (14.84 mm). No gender-related effect on MFC variability (i.e. MFC $\alpha$) was however identified.

<table>
<thead>
<tr>
<th>Variables</th>
<th>Women</th>
<th>Men</th>
<th>p-value</th>
</tr>
</thead>
<tbody>
<tr>
<td>MFC mean (mm)</td>
<td>11.63 ± 2.59</td>
<td>14.84 ± 1.76</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>MFC $\alpha$</td>
<td>0.84 ± 0.09</td>
<td>0.79 ± 0.09</td>
<td>0.088</td>
</tr>
</tbody>
</table>

**Table 2. MFC gait variables of the women and men participants**

* MFC mean - the average minimum foot clearance during walking;
* MFC $\alpha$ - scaling exponent $\alpha$ of the minimum foot clearance during walking.
Chapter 4. Discussion

The primary aim of the present study was to examine older adults’ gender-related differences in MFC, particularly regarding its MFC mean and MFC $\alpha$. As hypothesised, women presented smaller MFC mean than men, however the second hypothesis was refuted, since there were no significant differences in the complexity of MFC between sexes.

The overall MFC mean of all participants was 13.12 mm, which is consistent with Barrett, Mills, and Begg (2010) who reported values ranging between 10-20 mm. The dispersion in these values has been related with the type of methods and population used. For instance, Begg et al. (2007) used a geometric model with two markers (greater toe and metatarsal head) and a virtual point, to predict the lowest point on the shoe, while inertial sensors were used, in level walking, to calculate MFC (Hamacher, Hamacher, & Schega, 2014). Different types of footwear (A. M. Davis, B. Galna, A. T. Murphy, C. M. Williams, & T. P. Haines, 2016) and shoes with different rocker angles (Thies, Price, Kenney, & Baker, 2015) also impacts MFC values. Regarding the population Santhiranayagam, Lai, Sparrow, and Begg (2015) evaluated the MFC in young and old people, while others evaluated MFC in healthy elderly women (Karst, Hageman, Jones, & Bunner, 1999).

To the authors knowledge no studies compared MFC across gender, and from the studies available a median MFC of 13.8 mm was reported for elderly men (Mills et al., 2008), which is a little lower than the median (i.e. 14.80 mm) of the present study. Regarding to elderly females our results are similar to Khandoker et al. (2010) and Karmakar et al. (2013) that showed mean MFC values of 10.60 mm and 12.50 mm respectively. Therefore, the values of the present research seem to be in the scope of the current literature.

One possible reason for women to have a lower MFC than men can be associated to the fact that females during mid-swing of gait have higher gastrocnemius activation, a strategy that allows to maintain postural stability at the expense of energy efficiency (Bailey et al., 2018). Another reason can be related to the knee joint flexion angle, since women has been reported to show lower angles from late stance to mid-swing compared to men (Wilson et al., 2015). However, this last study should be interpreted carefully since the population showed some knee impairment and was submitted to arthroplasty surgery.

Human movement variability is intrinsic to the living being (Stergiou et al., 2016). Due human variability, the MFC will be different for each step during walking. Considering the small distance to the ground during the MFC, the margin for errors is very small, therefore the control of step-to-step variability must be tightened to avoid touching the ground and tripping, particularly in individuals with reduced MFC. However, individuals with high MFC can
be more prone to fall than individuals with lower MFC, if the former show greater variability of MFC than the latter. Furthermore, excess of variability in MFC can lead to incorrect ground foot contact, impacting the risk of fall (Khandoker, Palaniswami, & Begg, 2008).

Gender differences were reported in joint variability, when comparing young men and women, particularly women had less variability in several joint rotations than men (Barrett, Noordegraaf, & Morrison, 2008). However, these gender differences were not found in the present study regarding the MFC variability, because no gender-related effect on MFC scaling exponent $\alpha$ was observed.

The observed results of MFC $\alpha$ for women was (0.84) and for men was (0.79). These values exhibit persistent correlations in the stride interval time series. According to Goldberger et al. (2002) when the scaling exponent $\alpha$ is between 0.7 and 1.2, we are in the presence of a biological system that shows characteristics of adaptability. Therefore, the present results suggest that both men and women are in an interval which can be considered healthy in the sense that their movements are not too unstable or rigid but show adaptable capabilities. Additionally, the analysis of DFA in the MFC time series was performed with more than 600 data points, which allows a greater robustness of results when compared to other studies (Delignieres et al., 2006; Khandoker, Taylor, Karmakar, Begg, & Palaniswami, 2008). The absence of differences in DFA may be related to the study sample, since both men and women were physically active and performed exercise sessions regularly therefore the results might reflect their actual and healthier condition.

There are many strategies that can be used to minimize the risk of falls, for instance increase the mean MFC height, reduce the MFC variability (even though this may not be totally possible voluntarily and/or without training) and/or combine strategies (Begg et al., 2007). Regarding the outcomes of the present study the regulation of the MFC variability don’t seems to play an effective role in this population. On the other hand, the greater mean MFC height in men compared to women may simply be due restrictions/declines on women motor system and not a strategy pursued by men. Nevertheless, the reduced mean MFC height found in women can have a deleterious effect in the risk of fall when compared with men.

Some limitations should also be recognized: 1) data were recorded in the laboratory on a treadmill, although this method provides a direct measure of the MFC, walking changes are expected to occur when compared to normal walk in the ground; 2) another limitation is the interference of participants’ fatigue in the results, which, cannot be ruled out, even though all participants walked at their preferred speed and were submitted to the same procedure.
Chapter 5. Conclusion

In conclusion, although men and women had similar complexity of minimum foot clearance, women exhibited an average MFC lower than men, which may increase their risk of falling. The understanding of MFC and its complexity are relevant to promote appropriate interventions to reduce the risk of falls and to improve the quality of life in the elderly population.
Chapter 6. Future Research

Future investigations should try to understand if these gender differences also occur with:

1) young ages and different speeds;

2) on different surfaces and when in the presence of obstacles.

Population with higher risk of falls should also be compared to fully understand the scope of the present results. Specific fitness training plans targeted at older women might be developed and tested to minimize the decrease in the MFC mean.
Chapter 7. References


